

ASIM
A PET Analytical Simulator
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SimSET/Asim user group meeting
26 October, 2011
Valencia, Spain

a Non Monte Carlo Simulator

- Goal

Simulator for whole-body and dynamic PET imaging

- Applications

Test statistical methods, based on multiple realizations of a same scan

- Requirements

- Rapid

- Realistic Noise and Resolution Properties

Three-step simulation

- I) Analytical calculation: *simul*
 - true un-scattered coincidences
 - scattered coincidences
 - random coincidences
- II) Add noise to simulate the raw data: *noise*
 - prompt coincidences
 - delayed coincidences
- III) Same correction procedures as used in practice:
normalize

Accurate simulation of

- ⊗ the detection in the crystals
- ⊗ the random and scattered coincidences
- ☺ the noise properties for the corrected data

Emission and attenuation description

- Geometric

Analytical 3D projection

prevent non-physical interactions with projections /
back-projections used in reconstructions

- Voxel-based approach

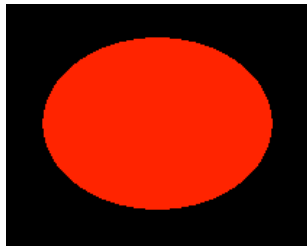
Numerical 3D projection

realistic morphological geometries (Zubal, MNI,
NCAT, ...)

Geometric description

Collection of truncated ellipsoids:

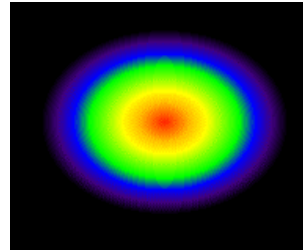
- emission density $e(\mathbf{x})$ [Bq/cc]
- linear attenuation coefficient $\mu(\mathbf{x})$ [1/cm]



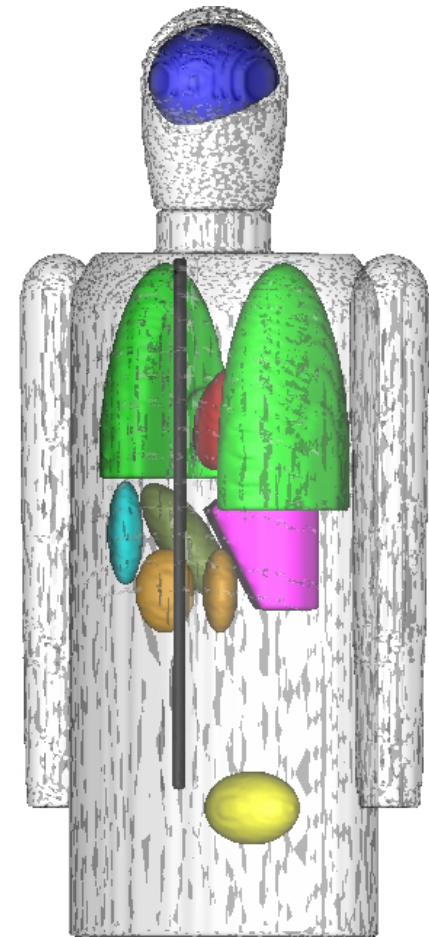
$e(\mathbf{x}), \mu(\mathbf{x})$



$e(\mathbf{x})$



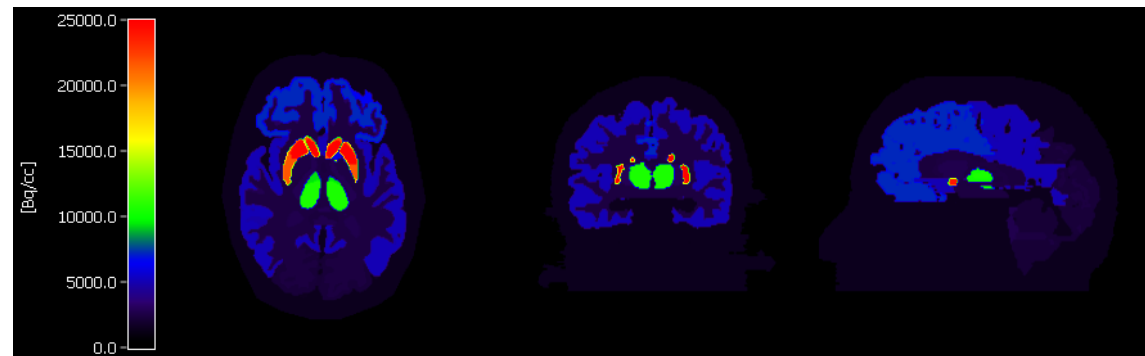
$e(\mathbf{x})$



Voxel-based description

3D numerical images:

- emission density e_i



- linear attenuation coefficient μ_i

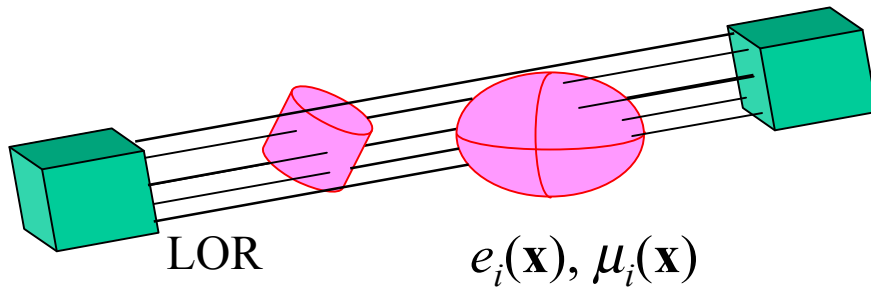


Analytic: Input parameters

- Phantom description, its offset and orientation
- Scanner model (cylindrical scanners)
- Multi-bed acquisition
 - Initial bed position
 - Number of bed positions
 - Amount of bed overlap
- Optional
 - normalization factors

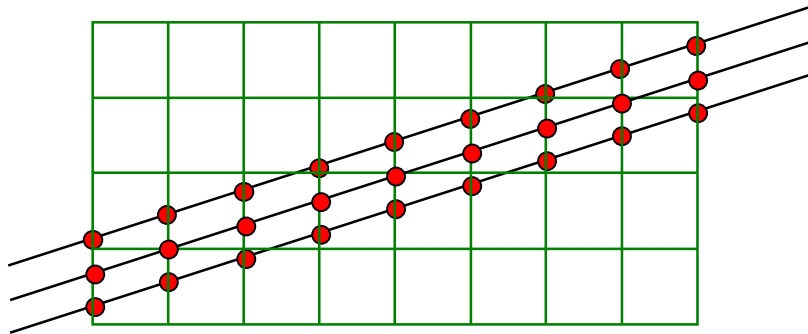
Analytic: True coincidences

normalization factors ε



$$t_E = \frac{AF}{\varepsilon} \sum_{\text{obj}_j \text{ LOR}} \int e_i(\mathbf{x}) dl$$

$$AF = e^{-\sum_{\text{obj}_j \text{ LOR}} \int \mu_i(\mathbf{x}) dl}$$



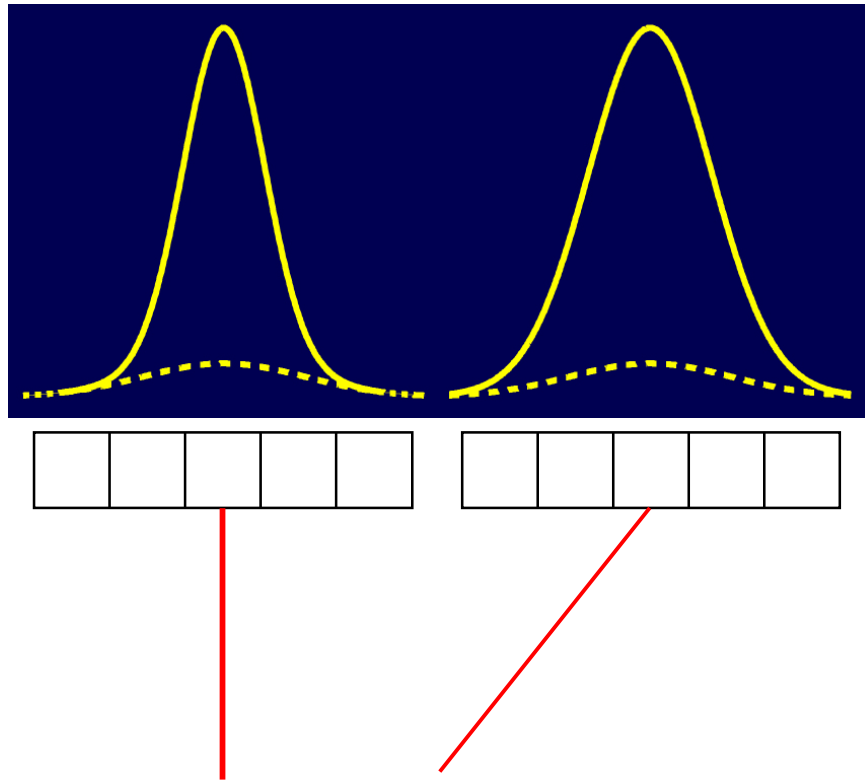
$$t_E = \frac{AF}{\varepsilon} \text{FwdProj}_{\text{LOR}} \{e_j\}$$

$$AF = e^{-\text{FwdProj}_{\text{LOR}} \{\mu_j\}}$$

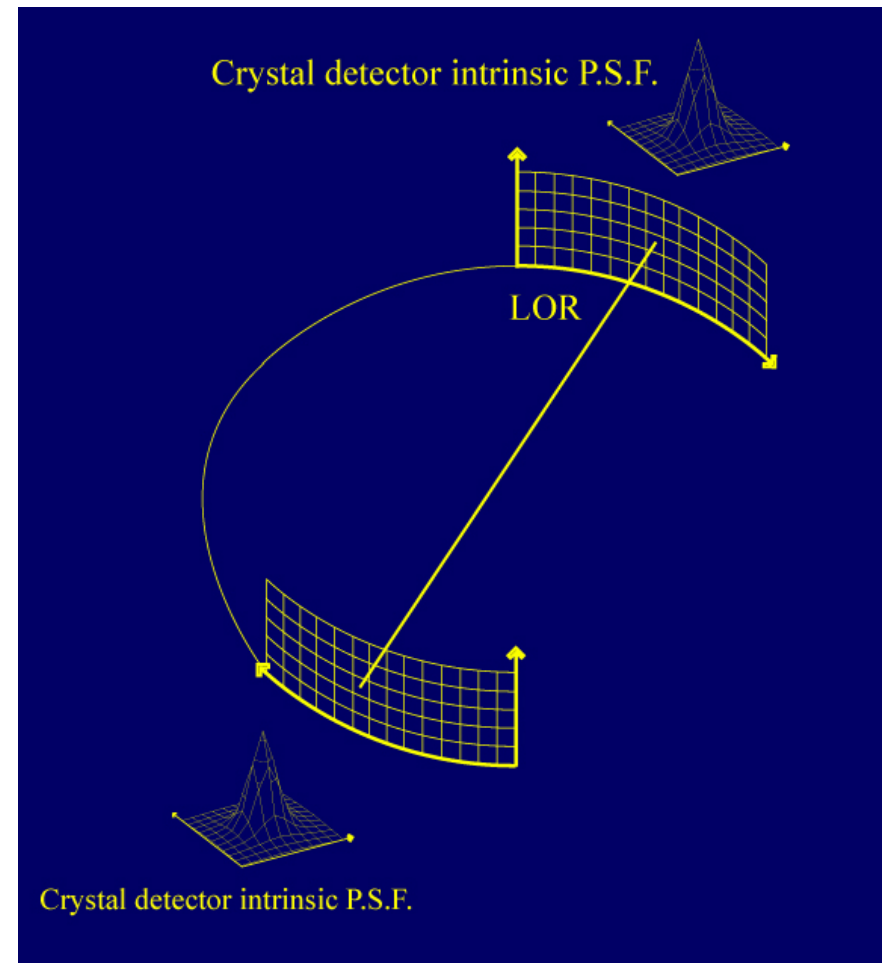
Ray driven 3D forward-projection

Intrinsic Scanner Resolution

Two 2-D convolutions by the crystal detector intrinsic P.S.F.



ASIM, an Analytical Simulator



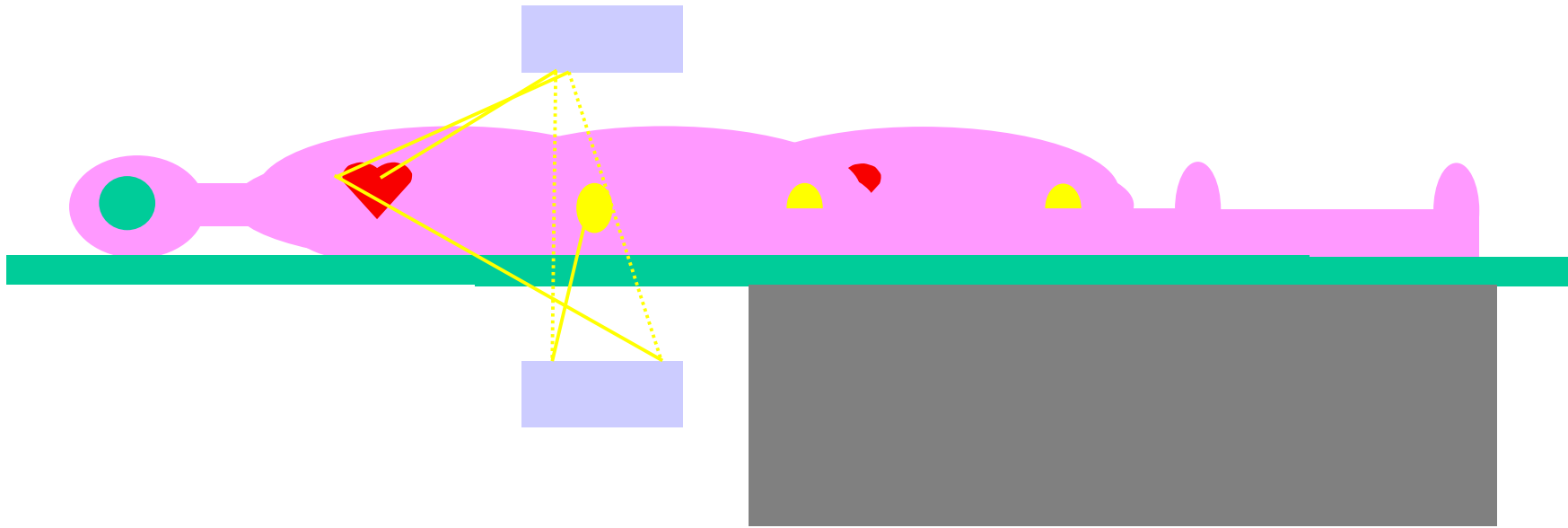
Valencia, 26 October, 2011

Analytic: Random & scatters

- Not accurate
- Effect on the noise of emission data
- Same analytical distribution to simulate the contamination and the correction term

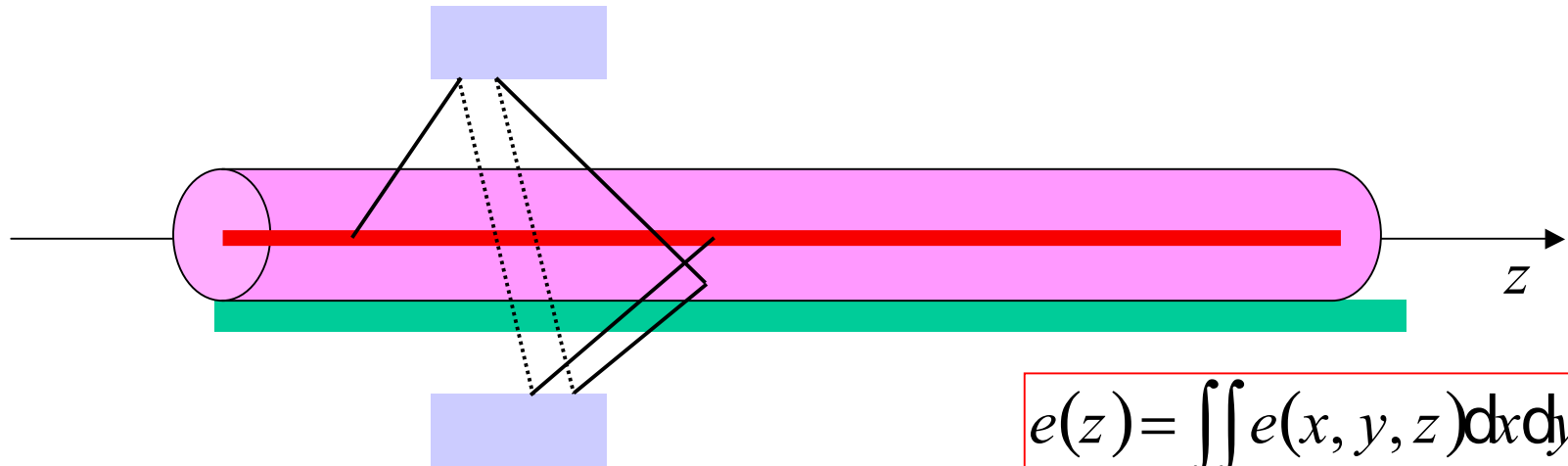
$\underbrace{\text{Poisson}[t_E + r_E + s_E]}_{\text{Prompt coincidences}} - \underbrace{\text{Poisson}[r_E] - s_E}_{\text{Delayed coincidences}}$	t_E	$t_E + 2 \cdot r_E + s_E$
	Mean	Variance
	$\underbrace{\text{Poisson}[t_E]}_{\text{True coincidences}}$	t_E

Activity outside FOV



	Brain	Heart	Liver
Scatters/Trues	0.3	1.0	0.8
Randoms/Trues	0.2	1.3	1.2

1D model

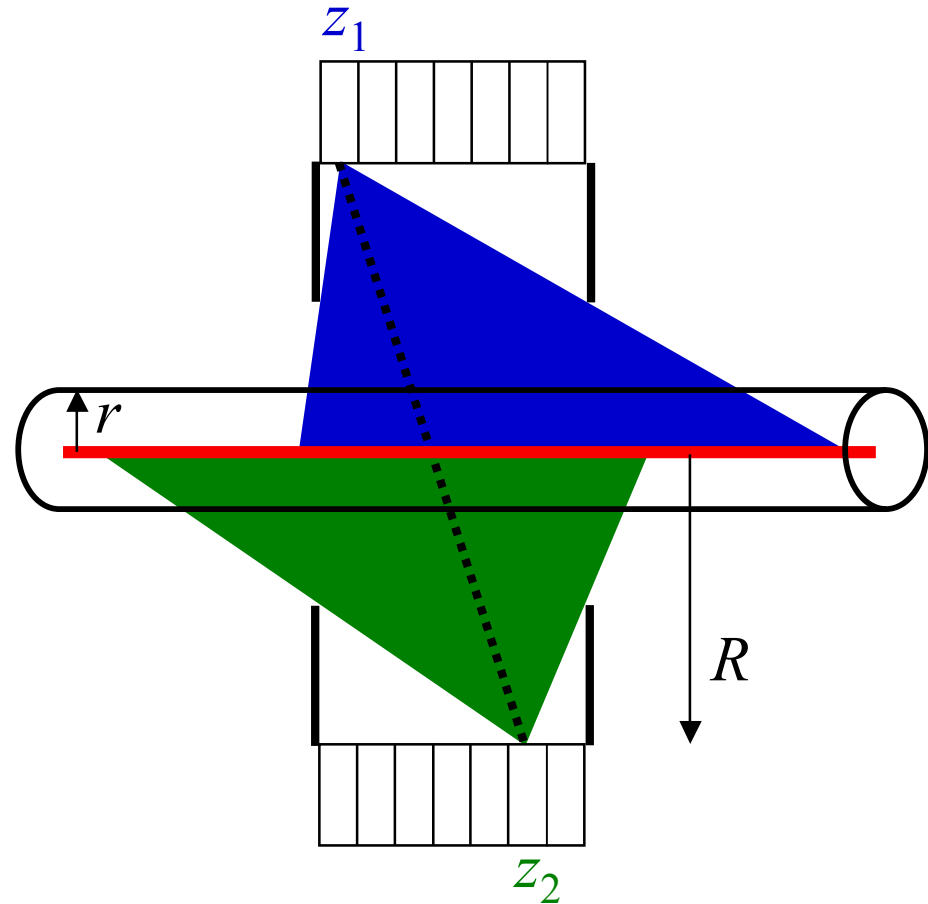


$$e(z) = \iint_{\perp} e(x, y, z) dx dy$$

$$r_E(s, \phi, z_1 + z_2, z_1 - z_2) = r_E^{\perp}(s) r_E''(z_1 + z_2, z_1 - z_2)$$

$$s_E(s, \phi, z_1 + z_2, z_1 - z_2) = s_E^{\perp}(s) s_E''(z_1 + z_2, z_1 - z_2)$$

Analytic Axial Random profile



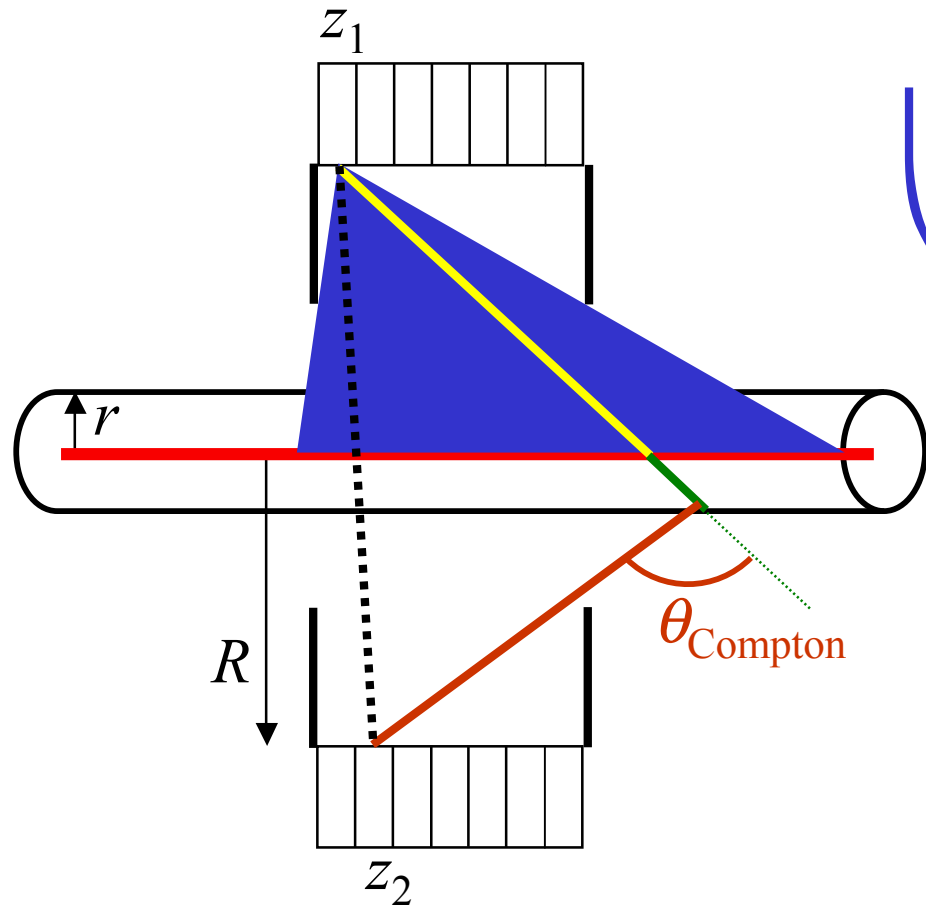
$$r_E''(z_1 + z_2, z_1 - z_2) =$$

$$\int_{z_{\min}(z_1)}^{z_{\max}(z_1)} \frac{e(z') \cdot e^{-r \sqrt{1 + \left(\frac{z' - z_1}{R}\right)^2} \mu}}{1 + \left(\frac{z' - z_1}{R}\right)^2} dz'$$

×

$$\int_{z_{\min}(z_2)}^{z_{\max}(z_2)} \frac{e(z'') \cdot e^{-r \sqrt{1 + \left(\frac{z'' - z_2}{R}\right)^2} \mu}}{1 + \left(\frac{z'' - z_2}{R}\right)^2} dz''$$

Analytic Axial Scatter profile



$$s_E''(z_1 + z_2, z_1 - z_2) =$$

Annihilation location

Compton scatter location

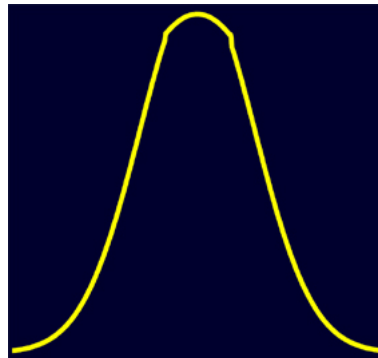
Compton scatter angle

⇒ Monte Carlo integration technique

Analytic scatter & random radial profiles

$$r_E^\perp(s), s_E^\perp(s)$$

- Not calculated
- Input to the simulation
 - 20-cm diameter cylinder scan
 - random: uniform profile
 - scatter: bell-shaped profile



Noise model

Analytical sinograms (true, random, and scattered coincidences)

- Arbitrary unit, does NOT predict the number of coincidences

Noise level

- Total numbers of true unscattered (N_{tE}), random (N_{rE}), and scattered (N_{sE}) coincidences for some range of bed positions $[b_1, b_2]$ or frames $[f_1, f_2]$

- Half-life of isotope $T_{1/2}$ ($\lambda = \ln 2 / T_{1/2}$)

- Scan duration Δt and start time t_b

$$DF_b = \frac{1 - e^{-\lambda \Delta t}}{e^{\lambda t_b} \cdot \lambda}$$

\Rightarrow calibration factors α_{tE} , α_{rE} , and α_{sE}

$$\alpha_{tE} \cdot \sum_{b=b_1}^{b_2} DF_b \sum_{s, \varphi, z_1, z_2} t_E(s, \varphi, z_1, z_2) = N_{tE}$$

Noise model

Alternatively

Noise level

- Calibration factors α_{tE} , α_{rE} , and SF
- Half-life of isotope $T_{1/2}$ ($\lambda = \ln 2 / T_{1/2}$)
- Scan duration Δt and start time t_b

$$\alpha_{tE} \cdot \sum_{b=b_1}^{b_2} DF_b \sum_{s, \varphi, z_1, z_2} t_E(s, \varphi, z_1, z_2) = N_{tE}$$

Full noise simulation

1) Acquired data

$$\tilde{p}_E = \text{Poisson}[\alpha_{tE} \cdot DF \cdot t_E + \alpha_{rE} \cdot DF' \cdot r_E + \alpha_{sE} \cdot DF \cdot s_E]$$
$$\tilde{d}_E = \text{Poisson}[\alpha_{rE} \cdot DF' \cdot r_E]$$

2) Corrections

$$\tilde{c}_E = \frac{\varepsilon}{\alpha_{tE} \cdot DF \cdot AF} (\tilde{p}_E - \tilde{d}_E - \alpha_{sE} \cdot s_E)$$

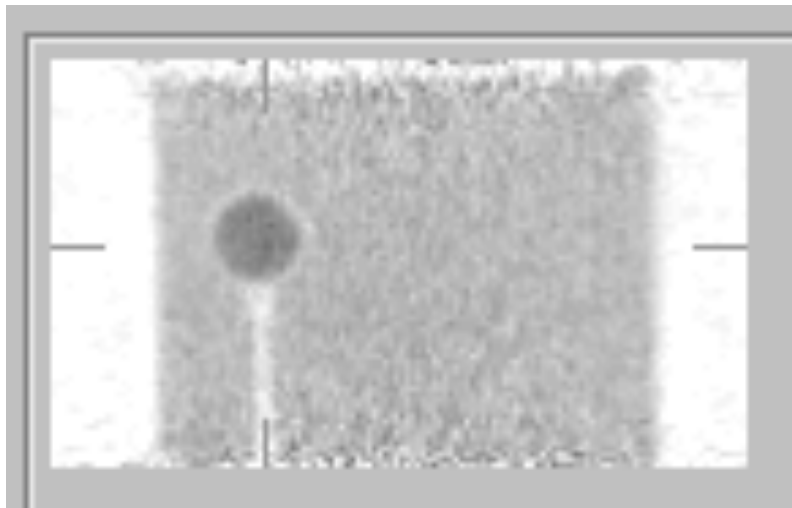
Use

Uses

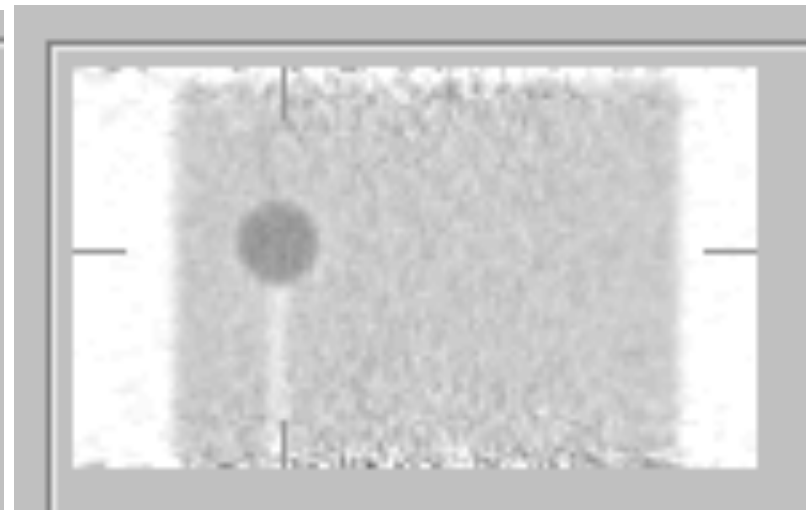
- Multiple realizations of a same acquisition
 - noise and SNR
 - human observer studies

Don't use:

- To evaluate Scatter correction techniques
- To predict Detector response



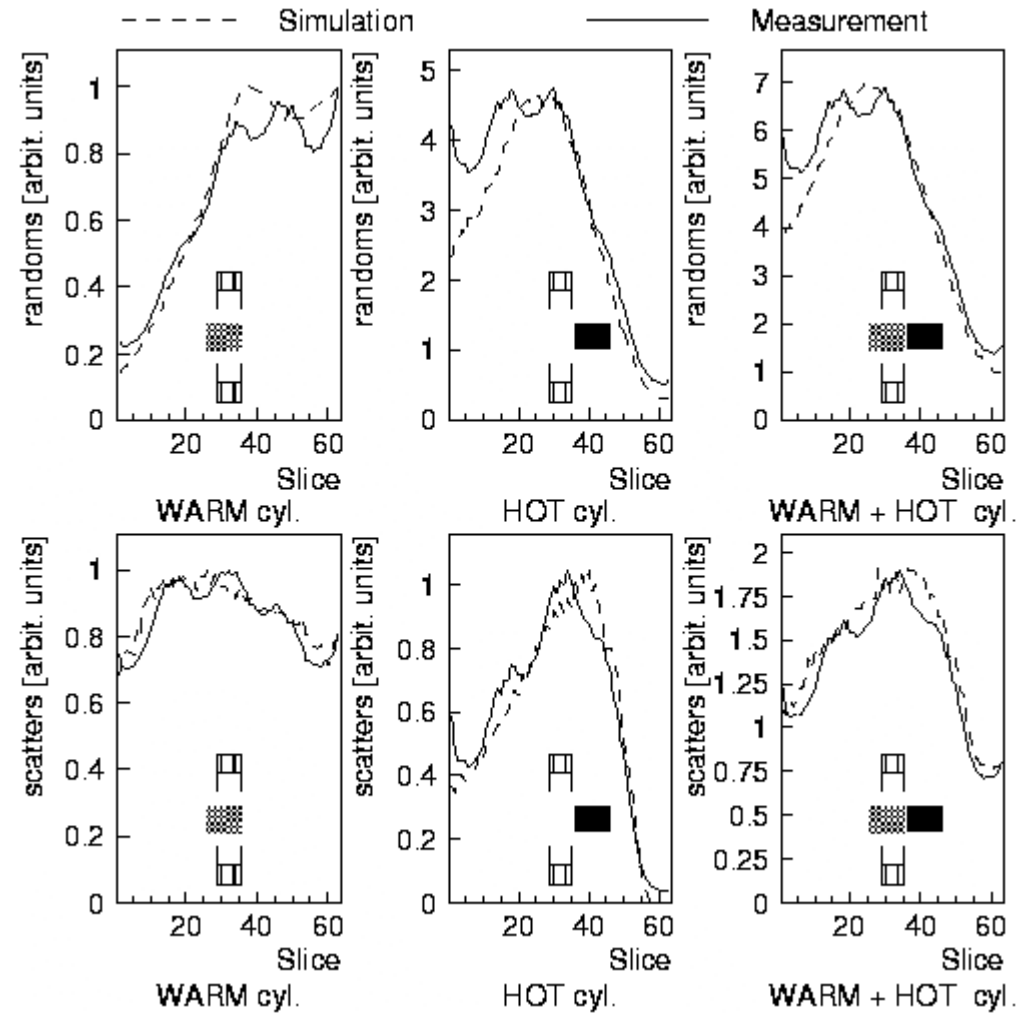
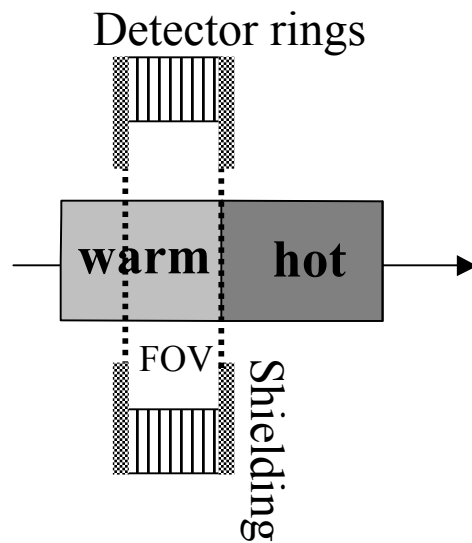
measured



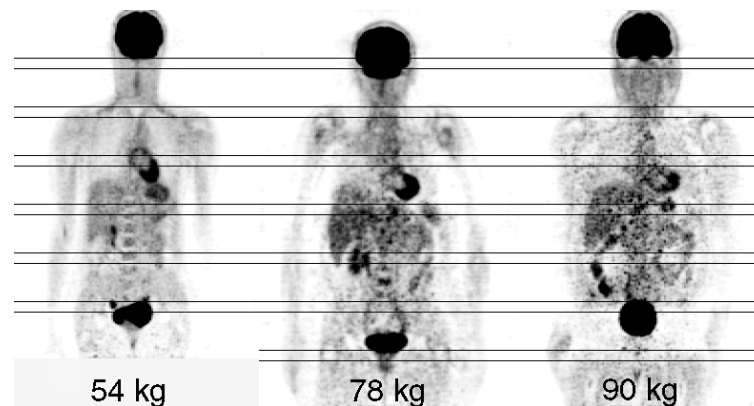
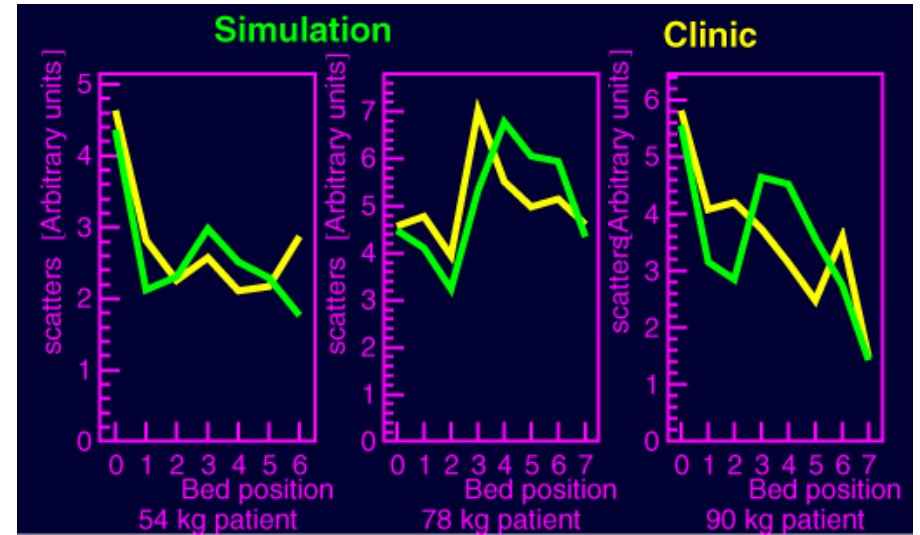
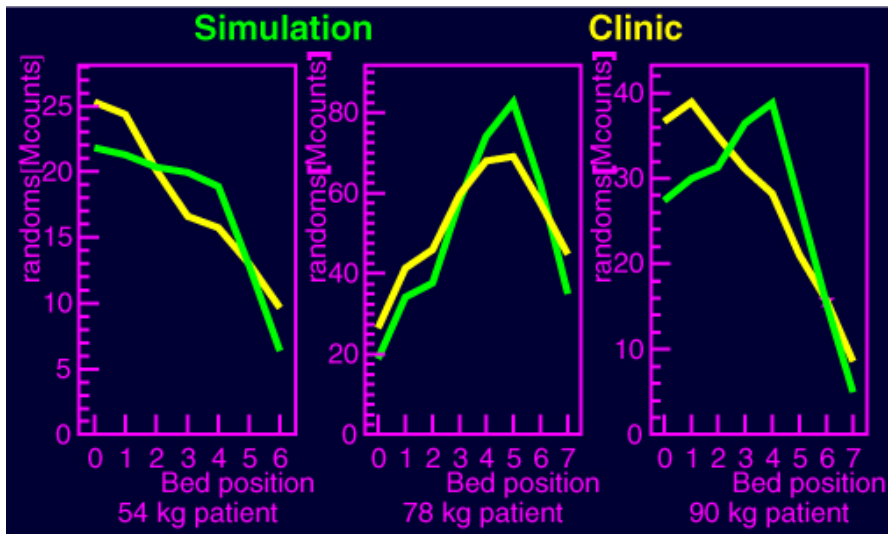
simulated



Scatter & random: comparison with cylinders

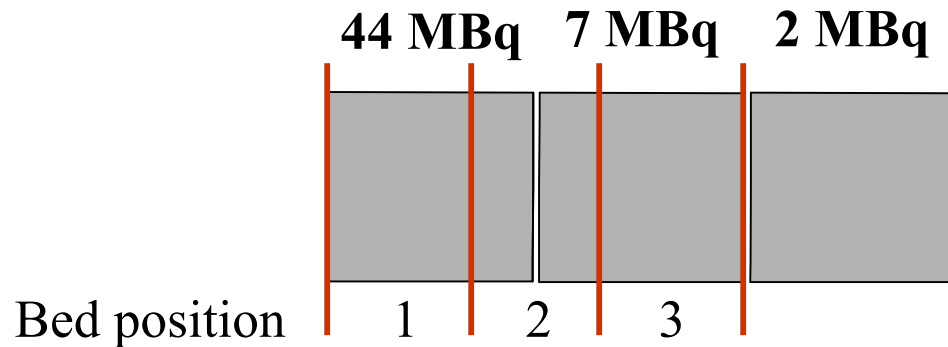
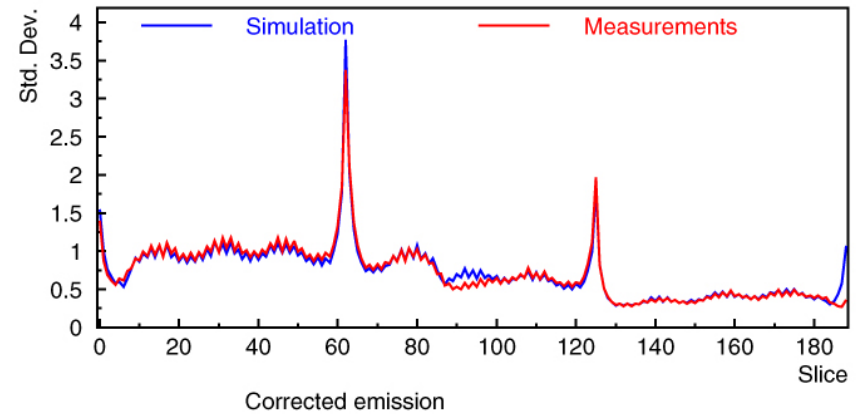
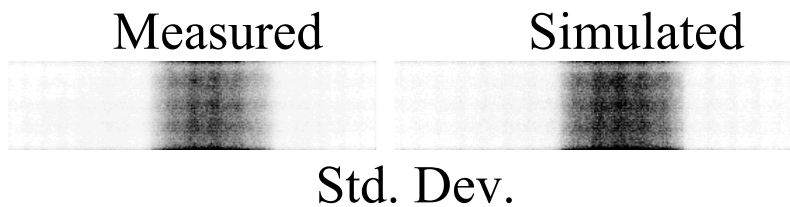


Scatter & random: comparison with patients



Validation

- Statistical distribution of the simulated events (c_E)



Gated acquisitions

Programs

1) simul

- analytic emission scan (t_E, s_E, r_E)
- voxelized image (to check geometric phantom)
- attenuation correction factors (ACF)
- run also under MPI

2) noise

- prompt and delayed emission data

3) normalize

- normalization factors
- scatter and random correction
- attenuation correction